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(54) OSTEOGENIC PASTE COMPOSITIONS AND USES THEREOF

OSTEOGENE PASTENZUSAMMENSETZUNGEN UND IHRE VERWENDUNG

COMPOSITIONS DE PÂTE OSTEOGENIQUE ET LEURS UTILISATIONS

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(73) Proprietor: **SDGI Holdings, Inc.
Wilmington, DE 19801 (US)**

(72) Inventor: **MCKAY, William, F.
Memphis, TN 38133 (US)**

(74) Representative: **Atkinson, Peter Birch et al
MARKS & CLERK,
Sussex House,
83-85 Mosley Street
Manchester M2 3LG (GB)**

(56) References cited:
**EP-A- 0 530 804 WO-A-89/04646
WO-A-93/16657 WO-A-96/39203
WO-A-96/40297 WO-A-97/40137
WO-A-98/17330 WO-A-98/40113
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Description

FIELD OF INVENTION

[0001] The present invention relates generally to osteogenic paste compositions containing a paste-form carrier and an osteogenic factor. In one specific aspect, this invention relates to osteogenic paste compositions containing a paste-form carrier, an osteogenic factor, and a substantial mineral component to provide a lasting scaffold for bone growth. Also described are methods of making and using the osteogenic paste compositions.

BACKGROUND

[0002] As further background, bone grafting is commonly used to augment healing in the treatment of a broad range of musculoskeletal disorders. Grafting has been effective in reconstruction or replacement of bone defects, to augment fracture repair, to strengthen arthrodeses and to fill defects after treatment of tumors. Autograft techniques have been known for over 100 years and include the use of cortical and cancellous bone as grafting material. The use of autografts presents several serious drawbacks including the limited amount of potential donor material available, the requirement for two surgical intrusion sites on the patient, a high incidence of donor site morbidity, the tedious and complex nature of the techniques, particularly when vascularized grafts are involved, and the fact that donated bone can rarely be precisely sized or shaped to fit the needs of the implant site. Allografts can also be used in analogous procedures. Allografts have the benefits of avoiding two-site surgery on the patient and the elimination of donor site morbidity risk. However, allografts have increased risks of disease transmission and immunogenic implant rejection. Procedures used to reduce these new risks inherently decrease the viability of the allografts as effective implant material. Procedures with allografts also remain tedious and complex, suffer from limited source material and have the same limitations on sizing and shaping the implant to optimally fit the needs of the implant site.

[0003] A number of compositions have been developed to augment or replace autographic and allographic techniques to reduce or avoid the above mentioned drawbacks. Ceramics such as hydroxyapatite, tricalcium phosphate (TCP), and coralline hydroxyapatite have been shown to be beneficial osteoconductive matrices for use as fillers and/or expanders in bone graft material. Ceramics can add compression strength, but lack osteoinductive properties and, when used alone, lack shear and tensile strength. R.W. Bucholz, A. Carlson, R.E. Holmes, *Hydroxyapatite and tricalcium phosphate bone graft substitutes*. Orthop. Clin. North Am., Vol. 18(2), 1987, pg. 323-334 and R.W. Bucholz, A. Carlson, R.E. Holmes, *Interporous hydroxyapatite as a bone graft substitute in tibial plateau fractures*, Clin. Orthop., Vol. 240,

1989, pg. 53-62. Further, it has been shown in animal studies, that such ceramics can be filled with marrow to provide a beneficial level of initial progenitor cells and other osteogenic factors. H. Ohgushi, V.M. Goldberg, A. I. Caplan, *Heterotopic osteogenesis in porous ceramics induced by marrow cells*, J. Orthop. Res., Vol. 7, 1989, pg. 568-578.

[0004] The calcium phosphate based ceramics differ widely in their resorption characteristics once implanted. In addition to other factors, the resorption rate tends to increase with surface area of the ceramic, which in turn depends on the ceramic's particle shape, size, density and porosity. TCP is degraded 10-20 times faster than hydroxyapatite. Also partly as a result, if new bone development is established with a TCP implant, the TCP is generally remodeled better than hydroxyapatite in the final stage of bone formation. It is noteworthy that TCP is resorbed by osteoclast cells, whereas, the much slower resorption of hydroxyapatite is effected mainly by foreign-body giant cells. The giant cells have a limit as to the amount of hydroxyapatite they will resorb.

[0005] Pure ceramics do not offer optimum handling characteristics during implantation, but do offer excellent biocompatibility properties and tend to bond well to the existing bone. Ohgushi, et al. teaches the use of marrow infiltration of ceramics, while others have used various binders with granulated ceramics to formulate workable pastes that solidify to provide stable implants of desired shape and size. C.P. Desilets, L.J. Marden, A.L. Patterson and J.O. Hollinger, *Development of synthetic bone-repair materials for craniofacial reconstruction*, J. Craniofacial Surgery, Vol. 1(3), 1990, pg. 150-153.

[0006] Demineralized bone matrix (DBM) preparations have been researched extensively for use as bone implant material. DBM is prepared through the acid extraction of minerals from bone. It includes the collagen matrix of the bone together with acid insoluble proteins including bone morphogenic proteins (BMPs) and other growth factors. DBM can be processed as crushed granules, powder or chips. It can be formulated for use as granules, gels, sponge material or putty and can be freeze-dried for storage. Sterilization procedures required to protect from disease transmission may reduce the activity of beneficial growth factors in the DBM. DBM provides an initial osteoconductive matrix and exhibits a degree of osteoinductive potential, inducing the infiltration and differentiation of osteoprogenitor cells from the surrounding tissues. DBM lacks structural strength and is therefore only useful to fill well supported, stable skeletal defects such as cysts, simple fractures, and fillers for autographs and allografts. Examples of commercially available DBM products are Grafton® Allogenic Bone Matrix by Osteotech, Shrewbury, NJ, and Dynagraft® by Gensci Regeneration Laboratories, Irvine, CA.

[0007] Various combinations of the above-mentioned bone implant materials have been made with a desire

to obtain the benefits of the individual components without their individual drawbacks. Some combinations have met with a measure of success, but Y. Yamazaki, S. Shioda and S. Oida, *Experimental Study on the Osteo-Induction Ability of Calcium Phosphate Biomaterials with added Bone Morphogenic Protein*, Transaction of the Society for Biomaterials, 1986, pg. 111, teach that not all combinations of elements known to be individually beneficial for bone implant materials are additive in their beneficial characteristics or effective as composite implant materials. Yamazaki, et al. found that the osteoinductive potential of DBM and osteogenic protein extracts therefrom are inhibited by the addition of TCP or hydroxyapatite. No osteogenic composition has yet been found to be optimum in generalized usage and clinical results vary widely, even with seemingly well defined compositions. There remains a need for improved osteogenic implant materials that are consistently strongly osteoinductive, osteoconductive, easily workable in surgical procedures, and that provide strength and stability for new bone formation during the early stages of bone development, but are essentially completely incorporated and remodeled into bone by the end of the osteogenic process.

[0008] Compositions of mixed ceramics of TCP/hydroxyapatite and collagen are commercially available and can be enhanced by filling with autogenous bone marrow prior to implant. The composites are available as pastes or soft strips and tend to flow away from the implant site. The implant must therefore be carefully retained in place until the composite and any surrounding bleeding has fully clotted.

[0009] Compositions of bone gel known as GRAFTON® (see U.S. Patent No. 5,481,601) comprising glycerol and DBM have been used singly and mixed with sand-like powder. Such compositions have been used to fill bone voids, cracks and cavities. GRAFTON® is available in flexible sheets or as a putty, thus making the composition more easily workable during implantation. Again, such compositions tend to flow away from the implant site.

[0010] Jefferies, in U.S. Patent 4,394,370 and 4,472,840, teach a bone implant material composition of collagen and DBM or solubilized BMP that is optionally crosslinked with glutaraldehyde.

[0011] Caplan et al., in U.S. Patent 4,620,327, describe the combination and partial immobilization by chemical cross-linking of soluble bone proteins with a number of solids to be implanted for bone repair/incorporation, including xenogenic bony implants, allografts, biodegradable masses and prosthetic devices to enhance new bone or cartilage formation. Ries et al., in U.S. Patent 4,623,553, describe the glutaraldehyde or formaldehyde cross-linking of collagen and hydroxyapatite or TCP. Ries does not include any osteoinductive elements and is deemed only osteoconductive.

[0012] Some researchers have suggested the use of composites of TCP and/or biopolymers like polylactide,

polyglycolide or their copolymers and particulate bone derivatives or BMP for craniofacial reconstruction. The TCP and biopolymers would provide a scaffold for new bone formation. The bone derivatives and BMP would induce osteogenesis beyond the slow, shallow osteoconduction induced by TCP and biopolymers alone. Desilets, et al.

[0013] Jefferies, in PCT WO 89/04646, describes osteoinductive implant materials having increased tensile strength by surface activating DBM or BMP with glutaraldehyde or other suitable cross-linking agent, followed by addition to a porous solid matrix where the activated DBM or BMP reacts with the solid to increase the cohesive strength of the composite. Jefferies also teaches the incorporation of therapeutic drugs into the matrix for the slow beneficial release thereof during the course of treatment.

[0014] In light of this background, there remain needs for improved osteogenic compositions and methods that effectively induce and support bone growth in mammals, including humans. The present invention is addressed to these needs.

SUMMARY OF THE INVENTION

[0015] The present invention generally provides osteogenic paste compositions including a paste-form carrier such as a gelatin paste and at least one osteogenic factor such as BMP-2 or another similar bone morphogenetic protein. A particular feature of the present invention relates to the discovery that the inclusion of an osteoblast- and osteoclast-stimulating osteogenic factor in a paste-form composition including a resorbable paste carrier causes a rapid and premature resorption of the carrier. This rapid resorption of the carrier can diminish or eliminate the capacity of the paste-form composition to effectively stimulate and support new bone formation in a void filled with the composition. This is particularly the case in primates, including humans, in which the rate of new bone formation is relatively slow.

[0016] Accordingly, one preferred embodiment of the present invention provides an osteogenic paste composition effective for the induction and support of new bone growth in a primate. The implant composition comprises a resorbable paste-form carrier, including for instance a paste made with a substance such as gelatin, hyaluronic acid, and/or carboxymethyl cellulose. The composition also includes an effective amount of an osteogenic factor, such as a bone morphogenetic protein, that stimulates both osteoblast cells and osteoclast cells. In addition, composition includes a substantial proportion of a particulate mineral that is effective to provide a scaffold for bone ingrowth when the resorbable paste carrier is resorbed at an increased rate due to the stimulation of osteoclast cell activity. Preferred such compositions of the invention are provided wherein the resorbable paste carrier includes gelatin, and/or wherein the resorbable paste carrier is flowable at temperatures above the body

temperature of the mammal in which it is to be implanted, but transitions to a relatively non-flowable mass at or slightly above said body temperature.

[0017] Importantly, the particulate mineral matrix constitutes a substantial proportion of the paste composition as a whole, in order to provide an effective scaffold for bone ingrowth. In most cases, the particulate mineral have an average particle size between about 0.050 and about 5.0 mm, and will constitute about 20% to 80% by volume of the overall composition, more typically higher levels of about 40% to about 80% by volume. The particulate mineral can include, for example, a natural or synthetic mineral, e.g. a material selected from the group consisting of bone particles, Bioglass®, tricalcium phosphate, hydroxyapatite, biphasic calcium phosphate, coralline hydroxyapatite, biocompatible ceramic and non-resorbable biocompatible organic polymer. Biphasic calcium phosphate is a particularly preferred synthetic ceramic for use in the present invention, advantageously having a tricalcium phosphate:hydroxyapatite weight ratio of about 80:20 to about 90:10.

[0018] In some preferred modes of carrying out the invention, the mineral comprises cancellous or cortical bone particles having an average particle size between about 0.050 and about 5.0 mm. Such bone particles can be of human or non-human (e.g. bovine) origin. In other modes, the mineral comprises tricalcium phosphate, biphasic calcium phosphate or hydroxyapatite having a particle size of about 0.50 to about 5.0 mm. In still another aspect of the invention, the paste composition further comprises demineralized bone matrix. The weight ratio of demineralized bone matrix to resorbable carrier is preferably between about 1:4 and about 3:2, respectively.

[0019] In one particularly preferred form of the present invention, an osteogenic paste composition for the induction of new bone growth in a primate is provided, comprising:

- (a) a resorbable paste carrier comprising gelatin, the resorbable paste carrier formulated to be flowable at temperatures above the body temperature of the primate, and to transitions to a non-flowable mass at such body temperature;
- (b) demineralized bone matrix;
- (c) a bone morphogenic protein that stimulates osteoblasts and osteoclasts, more preferably BMP-2 or BMP-7; and
- (d) cortical or cancellous bone particles, having an average particle size of between about 0.050 and about 5.0 mm, and constituting about 20% to about 80% by volume of the overall implant composition.

[0020] The present invention provides an improved osteogenic implant material that is strongly osteoinductive and that can be formed into precise shapes either prior to implant or during the surgical procedure itself. The present invention also provides implant materials

that retain stable shapes at the implant site and do not deform, migrate, or flow away from the implant site before ossification is established. Significantly, the present invention also provides advantageous implant materials that have enhanced osteoinductive potential and provide a matrix that is workable during implantation, but not resorbed prior to the establishment of bone within the void to be filled. Such preferred compositions provide a mineral scaffold for the generation of new bone that is subsequently incorporated into the bone matrix as the new bone matures. These and other objects, features and advantages of the present invention will be readily apparent from the following description.

15 BRIEF DESCRIPTION OF FIGURES

[0021]

Figure 1 shows ex vivo alkaline phosphatase activity as a function of time for intramuscular rat implants of demineralized bone matrix, a paste of gelatin and demineralized bone matrix, and of rhBMP-2 in each of a collagen sponge, a paste of gelatin and demineralized bone matrix, and in a paste of gelatin alone.

Figure 2 shows calcium content of explanted ossicles as a function of time for intramuscular rat implants of demineralized bone matrix, a paste of gelatin and demineralized bone matrix, and of rhBMP-2 in each of a collagen sponge, a paste of gelatin and demineralized bone matrix, and in a paste of gelatin alone.

35 DESCRIPTION OF THE PREFERRED EMBODIMENTS

[0022] For the purpose of promoting an understanding of the principles of the invention, reference will now be made to certain embodiments thereof and specific language will be used to describe the same. It will nevertheless be understood that no limitation of the scope of the invention is thereby intended, such alterations, further modifications and applications of the principles of the invention as illustrated herein being contemplated as would normally occur to one skilled in the art to which the invention relates.

[0023] As indicated above, the present invention generally provides osteogenic paste compositions including a paste-form carrier and a bone-growth-inducing amount of an osteogenic factor such as a bone morphogenic protein (BMP). The present invention features osteogenic paste compositions effective for use in primates, wherein the compositions exhibit high osteoinductive potential and provide a lasting mineral scaffold to support bone ingrowth. Such preferred compositions include a resorbable paste-form carrier, for example an aqueous paste including gelatin, and an osteogenic fac-

tor that stimulates the action of both osteoblasts (which biologically facilitate the formation of bone) and osteoclasts (which biologically facilitate the resorption of bone). In accordance with the present invention, it has been found that the incorporation of effective inductive amounts of such osteogenic factors, for example bone morphogenetic proteins, stimulates osteoclasts to such a level that the resorbable carrier is too quickly resorbed and, in the absence of a high mineral component in the composition, causes the performance of the composition to suffer in some cases to the extent that the observance of substantial bone ingrowth is sporadic.

[0024] Accordingly, a feature of the present invention is the provision of a paste-form osteogenic composition that includes a substantial amount of a relatively slowly-resorbed mineral component that remains at the implant site after the carrier has been rapidly resorbed, in order to provide a scaffold for new bone formation that is not prematurely resorbed due to the osteoclastic potentiation by the bone morphogenic protein in the composition.

[0025] Generally speaking, compositions in accordance with the present invention are in paste form and comprise a resorbable carrier, especially a gelatin paste, and an osteogenic factor such as a BMP that stimulates osteoblasts and osteoclasts, e.g. BMP-2 or BMP-7, especially BMP-2. The preferred compositions of the invention also include a substantial proportion (i. e. at least about 20% by volume) of a particulate, porous mineral matrix dispersed within the carrier. Such compositions can also include other resorbable components, for example demineralized bone matrix.

[0026] As to the carrier, in accordance with the present invention, it will be biologically resorbable and will contribute to providing a paste form to the composition allowing its implantation and retention at the candidate site for bone ingrowth. Preferred carriers will include resorbable macromolecules from biological or synthetic sources, for example gelatin, hyaluronic acid carboxymethyl cellulose, collagen, peptides, and the like. In more preferred inventive forms, the resorbable carrier, especially gelatin, is formulated into the composition such that the composition is flowable at temperatures above the body temperature of the mammal into which the material is to be implanted, but transitions to be relatively non-flowable at or slightly above such body temperature. The resorbable carrier may be formulated into the composition so the flowable state is a liquid or a flowable gel, and the non-flowable state is a stable gel or solid. In certain embodiments of the invention, the resorbable carrier is gelatin derived from the species receiving the implant, while in others the gelatin is derived from a species other than that of the mammal receiving the implant.

[0027] As is well known, when gelatin is solubilized in warm or hot aqueous solutions, the molecules have little organization. However, as a gelatin solution is allowed to cool, the gelatin molecules intertwine into a three di-

mensional matrix and the viscosity of the solution increases. At a characteristic set temperature, a phase transformation changes the flowable solution into a non-flowable gel. The set time, set temperature and density of the resulting non-flowable mass are dependent on several factors including the concentration of gelatin, the molecular weight and the intrinsic viscosity of the gelatin molecules and on the pH of the composition. Other components of the composition can affect the set time and temperature as well. The shortest set times are typically at the isoelectric point of the gelatin molecules.

[0028] As indicated in the passages above, other carriers can be used instead of or in addition to gelatin, to provide the paste composition. Illustrative macromolecules for these purposes include, for example, hyaluronic acid, cellulose derivatives such as carboxymethyl cellulose, collagens, peptides and the like. These and other similar materials which function as resorbable thickening agents will be suitable, and their incorporation into compositions of the present invention will be within the purview of those ordinarily skilled in the field given the teachings herein.

[0029] Paste compositions of the invention may also include other potentially osteoinductive substances, including for example demineralized bone matrix (DBM). As is known in the field, DBM can be prepared by acid demineralization of bone and when so prepared contains, among other constituents, the collagen matrix of the bone and acid insoluble proteins. DBM has been shown previously to be mildly osteoinductive by itself and has a favorable porous matrix for the ingrowth of bone. Methods of producing DBM are known in the art and are, therefore not elaborated upon here (see for example U.S. Patent 5,405,390). In a preferred form, DBM having a particle size of between about 0.10 and about 1.00 mm will be incorporated within compositions of the present invention. The DBM can be derived from the same or a different mammalian species as that in which the implant material is to be used. When used, the DBM is preferably blended with the resorbable carrier in a weight ratio between about 1:4 and about 3:2 DBM to resorbable carrier. Commercially available preparations of DBM are suitable for use in the present invention provided they may be uniformly blended with the other elements of the composition.

[0030] As indicated above, preferred paste compositions of the invention also include an osteoinductive factor, such as an osteoinductive protein or a nucleotide sequence encoding an osteoinductive protein operably associated with a promoter (e.g. provided in a vector such as a viral vector), for example a bone morphogenetic protein or a gene encoding the same operationally associated with a promoter which drives expression of the gene in the animal recipient to produce an effective amount of the protein. The bone morphogenetic protein (BMP) in accordance with this invention is BMP-2, BMP-4, BMP-6 or BMP-7, more preferably rhBMP-2 or rhBMP-7, most preferably, rhBMP-2. Purified recombinant

BMPs are preferred for use in the inventive compositions for their provision of high osteoinductive potentials. BMP gene sequences and methods for producing recombinant and naturally-derived BMPs are known in the art, and for additional information on this subject reference may be made, for instance, to U.S. Patent Nos. 5,108,753; 5,187,076; 5,366,875; 4,877,864; 5,108,922; 5,116,738; 5,013,649; 5,106,748; and 4,294,753; and International Publication Nos. WO93/00432; WO94/26893; and WO94/26892. The osteoinductive factor may also be LIM mineralization protein (LMP) or a suitable vector incorporating a gene encoding the same operably associated with a promoter, as described in WO99/06563 (see also genbank accession No. AF095585). When such vectors are employed as osteogenic factors in accordance with the invention, they are preferably delivered in conjunction with cells, for example autologous cells from the recipient of the implant. Most preferably the vector is to be delivered in conjunction with autologous white blood cells derived from bone marrow or peripheral blood of the recipient.

[0031] The osteogenic factor will be incorporated in an amount which is effective to stimulate the formation of bone within the animal recipient. In more preferred compositions incorporating protein osteogenic factors, the osteogenic factor will be incorporated in a weight ratio of about 1:100 to about 1:1000 relative to the overall composition, more preferably about 1:100 to about 1:500. As will be understood, when the osteogenic factor comprises a nucleotide sequence, sufficient amounts of the delivery vehicle (vector) will be incorporated to cause significant transduction of cells, so as to cause the generation of sufficient protein at the site to induce bone formation.

[0032] The osteogenic factor may be incorporated into the paste in any suitable manner, for example by pre-impregnating the mineral particles with the osteogenic factor prior to blending with the paste carrier, by blending the factor with the carrier, or both. Alternatively or in addition, amounts of the osteogenic factor can be blended with the carrier/ mineral mixture immediately prior to implantation.

[0033] The porous mineral used in accordance with the preferred embodiments of the present invention includes a natural or synthetic mineral that is effective to provide a scaffold for bone ingrowth as the resorbable carrier and other more rapidly resorbed elements of the implant composition are resorbed. Illustratively, the mineral matrix may be selected from one or more materials from the group consisting of bone particles, Bioglass®, tricalcium phosphate, biphasic calcium phosphate, hydroxyapatite, coralline hydroxyapatite, and biocompatible ceramics. Biphasic calcium phosphate is a particularly preferred synthetic ceramic for use in the invention. Desirably, such biphasic calcium phosphate will have a tricalcium phosphate:hydroxyapatite weight ratio of about 50:50 to about 95:5, more preferably about 70:30 to about 95:5, even more preferably about 80:20 to

about 90:10, and most preferably about 85:15.

[0034] In another preferred aspect of the invention, the mineral matrix includes bone particles, possibly cancellous but preferably cortical, ground to provide an average particle diameter between about 0.050 and 5.0 mm. Both human and non-human sources of bone are suitable for use in the instant invention, and the bone may be autographic, allographic or xenographic in nature relative to the mammal to receive the implant. Appropriate pre-treatments known in the art may be used to minimize the risks of disease transmission and/or immunogenic reaction when using bone particles in the mineral matrix.

[0035] In one embodiment of the instant invention, xenogenic bone that has been pretreated to reduce or remove its immunogenicity is used to provide the porous mineral matrix in the implant composition. For example, calcining or deproteinizing of the bone can be used to reduce the risks of immunogenic reactions to the implant material.

[0036] The level at which the mineral is incorporated into the preferred mineral-enhanced compositions of the invention is important to the provision of beneficial osteoinductive properties to the compositions. In general, the minimum level of mineral is dependent on activity of the BMP in the composition; the higher the activity of the BMP, the greater the content of the mineral matrix required to counter the osteoclastic potentiation of the BMP. As the BMP concentration increases, so does the rate of resorption of the resorbable carrier and DBM if present. As a result, the mineral content must be sufficient to provide a scaffold for the ingrowth of new bone while not abrogating the structural integrity of the composition. The mineral should also be such that as the new bone matures, the mineral is made an integral part of the tissue matrix or is resorbed during remodeling of the new bone in the natural course of bone growth and development.

[0037] In a preferred form of the invention, the mineral constitutes about 20% to about 80% by volume of the composition, more preferably about 40% to about 80%. Generally speaking, the amount of mineral in the paste composition will be sufficient to provide a scaffold that will remain in the patient for a period of time sufficient for the formation of osteoid in the area for which bone growth is desired. Typically, this period of time will be about 6 to about 8 weeks.

[0038] As further enhancements of the compositions of the present invention, those skilled in the art will readily appreciate that other osteogenic enhancing factors may be incorporated into the composition. Such additional factors include, but are not limited to host compatible osteogenic progenitor cells, autographic bone marrow, allographic bone marrow, transforming growth factor-beta, fibroblast growth factor, platelet derived growth factor, insulin-like growth factor, microglobulin-beta, antibiotics, antifungal agents, wetting agents, glycerol, steroids and non-steroidal anti-inflammatory com-

pounds.

[0039] In use, the paste-form implant compositions of the invention are to be implanted at a site at which bone growth is desired, e.g. to treat a disease, defect or location of trauma, and/or to promote artificial arthrodesis. The paste form of the compositions enables their positioning, shaping and/or molding within voids, defects or other areas in which new bone growth is desired. In the case of implant compositions which are flowable at temperatures higher than the body temperature of the mammal in which they are to be implanted, yet which transition to a non-flowable mass at or near such body temperature, the composition is heated to a temperature at which it is flowable, but which will not denature any osteogenic factor present; molded or otherwise shaped to the shape of the desired new bone; cooled to a temperature sufficient to transition the osteogenic implant material into a non-flowable mass either in situ or implanted at the site of desired new bone formation after setting up. In other preferred situations, the paste composition does not require heating to above body temperature (about 37°C) for flowability, for example wherein the paste composition is flowable at temperatures below 37°C and cures or solidifies into a non-flowable mass upon heating or upon contact with a separate curing agent. Such cases are particularly advantageous in that heat-induced denaturation of the osteogenic factor is less of a concern.

[0040] Once in place, the paste form implant compositions of the invention will effectively induce and support the ingrowth of bone into the desired area even in a primate subject such as a human exhibiting a relatively slow rate of bone formation compared to smaller mammals, for example rodents or rabbits. In particular, while the paste carrier is generally resorbed relatively quickly, the substantial mineral component remains as a scaffolding to support new bone growth in and through the desired area. In this regard, it is preferred that the mineral matrix be chosen and included in an amount which will provide a scaffold which is detectable in the treated subject for a period sufficient for the formation of osteoid in the volume to be filled with bone, typically about 6 to about 8 weeks. This will facilitate effective bone formation even where the resorbable carrier and other quickly-resorbed components of the paste are rapidly eliminated from the implant site.

[0041] Compositions of the invention are especially advantageous when used in bones or bone portions that are vascularized to only moderate or low levels. These areas present particularly low rates of bone formation, and as such the rapid resorption of the carrier poses enhanced difficulties. Examples of moderate or only slightly vascularized sites include, for example, transverse processes or other posterior elements of the spine, the diaphysis of long bones, in particular the mid diaphysis of the tibia, and cranial defects

[0042] An especially preferred use of paste compositions of the invention is as an implant to promote arthro-

desis between vertebrae in spinal fusions in humans or other primates, including for example interbody, posterior and/or posterolateral fusion techniques. Although the rate of bone-formation in the primate spine is relatively slow overall and thus will benefit generally from the present invention, the elements to be fused in posterior and posterolateral fusions exhibit particularly low levels of vascularization and thus fusions of these elements are expected to benefit markedly from the invention. In addition, in accordance with other aspects of the invention, the osteogenic paste compositions of the invention can be incorporated in, on or around a load-bearing (e.g. having a compressive strength of at least about 10000 N) implant device such as a fusion cage, dowel, or other device having a pocket, chamber or other cavity for containing an osteogenic composition, and used in a spinal fusion such as an interbody fusion.

[0043] The invention will now be more particularly described with reference to the following specific Examples. It will be understood that these Examples are illustrative and not limiting of the invention.

EXAMPLE 1

Rat Study Comparing the Effect of rhBMP-2 on Osteogenic Capacity of a Matrix Consisting of Collagen Derived Gelatin and Demineralized Bone Matrix (DBM).

[0044] Thirty young adult male Sprague-Dawley rats weighing between 200-220 g, were randomly assigned to two groups. Each animal was surgically implanted with six 0.050 mL samples. The samples were inserted in pockets incised into the rectus abdominus muscles on either side of the midline. Samples were placed three to a side, evenly spaced in lines extending from below the sternum to above the mid-groin.

[0045] Two of the six samples for each animal were positive controls, one being DBM alone, the second being Helistat® Absorbable Collagen Sponge (ACS) onto which 0.004 mg rhBMP-2 had been adsorbed. Group I animals were also given duplicate samples of a gelatin/DBM injectable matrix (Gelatin Bone Paste) and duplicate samples of the Gelatin Bone Paste mixed with 0.001 mg rhBMP-2. Group II animals were given duplicate samples of the Gelatin Bone Paste mixed with 0.002 mg rhBMP-2 and duplicate samples of the gelatin without DBM (Gelatin) mixed with 0.002 mg rhBMP-2.

[0046] Five animals from each group were sacrificed at each time point of two, fourteen and twenty-one days. At sacrifice, the implant areas were excised and analyzed for alkaline phosphatase activity, radiography, bone density, histology and histomorphometry.

[0047] Figure 1 shows alkaline phosphatase activity in the samples. Increased activity is indicative of infiltration of the implants by osteoprogenitor cells. The timing and magnitude of increased activity is evidence of the osteoinductive potential of the implant. The Gelatin Bone Paste samples with rhBMP-2 exhibited earlier and

higher alkaline phosphatase activity peaks than the controls or the Gelatin Bone Paste alone. Surprisingly, the 0.001 mg rhBMP-2 samples gave higher activity peaks than did the 0.002 mg rhBMP-2 samples.

[0048] Figure 2 shows the calcium content of the excised implants. Increased calcium content is indicative of bone formation. As with the alkaline phosphatase data, the Gelatin Bone Paste samples with rhBMP-2 outperformed both the controls and the Gelatin Bone Paste without rhBMP-2 samples in initiating calcification of the implant. It is again surprising that the 0.001 mg rhBMP-2 in Gelatin Bone Paste samples were more effective at initiating calcification than the 0.002 mg rhBMP-2 in Gelatin Bone Paste samples. It is also noteworthy that the twenty-one day samples of the higher concentration of rhBMP-2 showed a diminishing of calcification compared to the fourteen day samples.

[0049] These data are indicative of the osteoclastic potentiation of rhBMP-2 balancing its osteoblast stimulating properties; higher rhBMP-2 concentrations stimulate the resorption of the essentially collagen matrix, limiting the osteogenic potential of such matrices that do not incorporate mineral matrix elements to provide prolonged scaffolding for the bone formation process. It should be noted that the ACS controls containing 0.004 mg rhBMP-2 and the gelatin samples containing 0.002 mg rhBMP-2 had the most readily resorbable matrices and gave the poorest calcification performances for samples containing rhBMP-2. See figure 2.

EXAMPLE 2

Monkey Study Comparing Osteogenicity of rhBMP-2 Containing Implant Matrices.

[0050] Studies in a monkey spinal fusion model were conducted to determine the effectiveness of three paste compositions. The compositions were the gelatin bone paste of Example 1, that paste containing autograft bone chips, and that paste containing rhBMP-2 at a single level of the spine. Each composition was used in bilateral fusion of vertebra in rhesus monkeys and analyzed for its ability to induce new bone formation. In doing so, CT scans were taken every two months over a six-month period. The results demonstrated variable bone growth in monkeys receiving the paste of Example 1 alone and in the paste containing autograft bone chips, but no growth in monkeys receiving the paste and rhBMP-2. This observation is expected to be due to the premature resorption of the carrier in the rhBMP-2-containing paste, leaving no matrix for bone ingrowth. Accordingly, incorporation of a substantial mineral component in a BMP-containing paste in accordance with the present invention will provide a lasting matrix and scaffold for bone ingrowth, thus improving performance.

[0051] The invention has been described above in detail, with specific reference to its preferred embodiments. It will be understood, however, that a variety of

modifications and additions can be made to the procedures disclosed without departing from the scope of the invention.

Claims

1. An osteogenic paste composition effective for the induction of new bone growth in a primate, comprising:
 - a resorbable paste carrier;
 - an osteogenic factor which is a bone morphogenic protein selected from BMP-2, BMP-4, BMP-6 or BMP-7, a LIM mineralization protein, or a nucleotide sequence encoding said bone morphogenic protein or LIM mineralization protein; and
 - a porous particulate mineral constituting about 40% to 80% by volume of the composition, said amount being effective to provide a scaffold for bone ingrowth as a resorbable paste carrier is resorbed.
2. The composition of claim 1 which further comprises demineralised bone matrix.
3. The composition of claim 2 wherein the ratio of demineralised bone matrix to resorbable carrier is between about 1:4 and about 3:2 by weight.
4. The composition of claim 2 wherein the composition comprises 5-45% by weight resorbable carrier.
5. The composition of claim 1 wherein the resorbable carrier is flowable at temperatures above the body temperature of the mammal, but transitions to a non-flowable mass at or slightly above said body temperature.
6. The composition of claim 1 wherein the mineral is selected from the group consisting of bone particles, bioglass, tricalcium phosphate, hydroxyapatite, coralline hydroxyapatite, biocompatible ceramic and non-resorbable biocompatible organic polymer.
7. The composition of claim 1 wherein the mineral comprises tricalcium phosphate, biphasic calcium phosphate, or hydroxyapatite particles having an average particle diameter of about 0.050 to about 5.0 mm.
8. The composition of claim 1 wherein the mineral comprises mammalian bone particles having a particle size of about 0.050 to about 5.0 mm.
9. The composition of claim 1 wherein the mineral

comprises cortical human bone particles having an average particle diameter of about 0.050 to about 5.0 mm.

10. The composition of claim 1 further comprising one or more osteogenic enhancing factors selected from the group consisting of osteogenic progenitor cells, autographic bone marrow, allographic bone marrow, transforming growth factor-beta, fibroblast growth factor, platelet derived growth factor, insulin-like growth factor, microglobulin-beta, antibiotics, antifungal agents, wetting agents, glycerol, steroids and non-steroidal anti-inflammatory compounds.

11. An osteogenic implant material effective for the induction of new bone growth in a mammal, comprising:

a resorbable paste carrier comprising gelatin, the resorbable carrier formulated to be flowable at temperatures above the body temperature of the mammal, and to transition to a non-flowable mass at said body temperature;
demineralized bone matrix;
an osteogenic factor which is a bone morphogenic protein selected from BMP-2, BMP-4, BMP-6 and BMP-7, a LIM mineralization protein, or a nucleotide sequence encoding said bone morphogenic protein or LIM mineralization protein; and
a particulate mineral having an average particle size of about 0.050 to about 5.0 mm, said mineral constituting at least 20% by volume of said composition.

12. The composition of claim 11 wherein the mineral constitutes about 20% to about 80% by volume of the composition.

13. The composition of claim 11 wherein the mineral comprises human bone particles.

14. The composition of claim 11 wherein the mineral comprises non-human bone particles, said particles having been treated to reduce their immunogenicity in humans.

Patentansprüche

1. Eine osteogene Pastenzusammensetzung, wirksam zur Induktion von Knochenneuwachstum bei einem Primaten, umfassend:

einen resorbierbaren Pastenträger;
einen osteogenen Faktor, der ein knochenmorphogenetisches Protein ist, ausgewählt aus BMP-2, BMP-4, BMP-6 oder BMP-7, einem

LIM-Mineralisierungsprotein oder eine Nukleotidsequenz, die für das knochenmorphogenetische Protein oder das LIM-Mineralisierungsprotein codiert; und

ein poröses partikuläres Mineral, welches etwa 40 Vol.-% bis 80 Vol.-% der Zusammensetzung ausmacht, wobei die Menge wirksam ist, um ein Gerüst zum Knocheneinwuchs bereitzustellen, da ein resorbierbarer Pastenträger resorbiert wird.

2. Die Zusammensetzung nach Anspruch 1, welche weiterhin demineralisierte Knochenmatrix umfasst.

3. Die Zusammensetzung nach Anspruch 2, wobei das Gewichts-Verhältnis von demineralisierter Knochenmatrix zu resorbierbarer Trägersubstanz zwischen etwa 1:4 und etwa 3:2 liegt.

4. Die Zusammensetzung nach Anspruch 2, wobei die Zusammensetzung 5-45 Gew.-% resorbierbare Trägersubstanz umfasst.

5. Die Zusammensetzung nach Anspruch 1, wobei der resorbierbare Träger fließfähig ist bei Temperaturen oberhalb der Körpertemperatur des Säugers, aber übergeht zu einer nicht-fließfähigen Masse bei oder leicht oberhalb der Körpertemperatur.

6. Die Zusammensetzung nach Anspruch 1, wobei das Mineral ausgewählt ist aus der Gruppe bestehend aus Knochenpartikeln, Bioglass, Tricalciumphosphat, Hydroxyapatit, korallinem Hydroxyapatit, biokompatibler Keramik und nichtresorbierbarem biokompatiblen organischem Polymer.

7. Die Zusammensetzung nach Anspruch 1, wobei das Mineral Tricalciumphosphat, biphasisches Calciumphosphat oder Hydroxyapatit umfasst als Partikel mit einem durchschnittlichen Partikeldurchmesser von etwa 0,050 bis etwa 5,0 mm.

8. Die Zusammensetzung nach Anspruch 1, wobei das Mineral Knochenpartikel von Säugern umfasst mit einer Partikelgröße von etwa 0,050 bis etwa 5,0 mm.

9. Die Zusammensetzung nach Anspruch 1, wobei das Mineral humane kortikale Knochenpartikel umfasst mit einem durchschnittlichen Partikeldurchmesser von etwa 0,050 bis etwa 5,0 mm.

10. Die Zusammensetzung nach Anspruch 1, weiterhin umfassend einen oder mehrere Osteogenese-fördernde Faktoren ausgewählt aus der Gruppe bestehend aus Osteoprogenitorzellen, autologem Knochenmark, allogem Knochenmark, transformierendem Wachstumsfaktor-Beta, Fibroblasten-

Wachstumsfaktor, Plättchen-Wachstumsfaktor (PDGF), Insulinartigem Wachstumsfaktor, Beta-Mikroglobulin, Antibiotika, Antipilzmitteln, Netzmitteln, Glycerin, Steroiden und nichtsteroidalen antientzündlichen Verbindungen.

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11. Ein osteogenes Implantatmaterial wirksam zur Induktion von Knochenneuwachstum in einem Säuger, umfassend:

einen resorbierbaren Pastenträger umfassend Gelatine, wobei der resorbierbare Träger derartig formuliert ist, um bei Temperaturen oberhalb der Körpertemperatur des Säugers fließfähig zu sein und bei Körpertemperatur zu einer nicht-fließfähigen Masse überzugehen; demineralisierte Knochenmatrix; einen osteogenen Faktor, welcher ein knochenmorphogenetisches Protein ist, ausgewählt aus BMP-2, BMP-4, BMP-6 und BMP-7, einem LIM-Mineralisierungsprotein oder einer Nukleotidsequenz, die für das knochenmorphogenetische Protein oder das LIM-Mineralisierungsprotein codiert; und ein partikuläres Mineral mit einer durchschnittlichen Partikelgröße von etwa 0,050 bis etwa 5,0 mm, wobei das Mineral mindestens 20 Vol.-% der Zusammensetzung ausmacht.

12. Die Zusammensetzung nach Anspruch 11, wobei das Mineral etwa 20 Vol.-% bis etwa 80 Vol.-% der Zusammensetzung ausmacht.

13. Die Zusammensetzung nach Anspruch 11, wobei das Mineral humane Knochenpartikel umfasst.

14. Die Zusammensetzung nach Anspruch 11, wobei das Mineral nicht-humane Knochenpartikel umfasst, wobei die Partikel behandelt worden sind, um ihre Immunogenität in Menschen zu reduzieren.

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Revendications

1. Composition de pâte ostéogénique efficace pour induire une nouvelle croissance osseuse chez un primate, comprenant:

un support de pâte résorbable;

un facteur ostéogénique qui est une protéine morphogénique osseuse choisie parmi BMP-2, BMP-4, BMP-6 ou BMP-7, une protéine de minéralisation LIM ou une séquence nucléotidique codant ladite protéine morphogénique osseuse ou protéine de minéralisation LIM; et

un minéral particulaire poreux constituant envi-

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ron 40% à 80% en volume de la composition, cette quantité étant efficace pour procurer une charpente pour un développement osseux à mesure qu'un support de pâte résorbable se résorbe.

2. Composition selon la revendication 1, qui comprend en outre une matrice osseuse déminéralisée.

3. Composition selon la revendication 2, dans laquelle le rapport de la matrice osseuse déminéralisée au support résorbable est entre environ 1:4 et environ 3:2 en poids.

4. Composition selon la revendication 2, la composition comprenant 5-45% en poids de support résorbable.

5. Composition selon la revendication 1, dans laquelle le support résorbable est fluide à des températures au-dessus de la température corporelle du mammifère, mais se transforme en une masse non fluide à ladite température corporelle ou légèrement au-dessus de celle-ci.

6. Composition selon la revendication 1, dans laquelle le minéral est choisi dans le groupe constitué par les particules osseuses, le bioverre, le phosphate tricalcique, l'hydroxyapatite, l'hydroxyapatite de coralline, une céramique biocompatible et un polymère organique biocompatible non résorbable.

7. Composition selon la revendication 1, dans laquelle le minéral comprend des particules de phosphate tricalcique, de phosphate calcique biphasique ou d'hydroxyapatite ayant un diamètre moyen de particule d'environ 0,050 à environ 5,0mm.

8. Composition selon la revendication 1, dans laquelle le minéral comprend des particules d'os mammifère ayant une taille de particule d'environ 0,050 à environ 5,0mm.

9. Composition selon la revendication 1, dans laquelle le minéral comprend des particules d'os humain cortical ayant un diamètre moyen de particule d'environ 0,050 à environ 5,0mm.

10. Composition selon la revendication 1, comprenant en outre un ou plusieurs facteurs activateurs ostéogéniques choisis dans le groupe constitué par les cellules progénitrices ostéogéniques, une autogrefe de moelle osseuse, une allogrefe de moelle osseuse, le facteur de croissance transformant bêta, le facteur de croissance des fibroblastes, le facteur de croissance plaquettaire, le facteur de croissance semblable à l'insuline, la microglobuline-bêta, les antibiotiques, les agents antifongiques, les agents

mouillants, le glycérol, les stéroïdes et les composés anti-inflammatoires non stéroïdiens.

11. Matériau d'implant ostéogénique efficace pour induire une nouvelle croissance osseuse chez un mammifère, comprenant: 5

un support de pâte résorbable comprenant de la gélatine, le support résorbable formulé pour être fluide à des températures supérieures à la température corporelle du mammifère, et se transformer en une masse non fluide à ladite température corporelle; 10

une matrice osseuse déminéralisée; 15

un facteur ostéogénique qui est une protéine morphogénique osseuse choisie parmi BMP-2, BMP-4, BMP-6 et BMP-7, une protéine de minéralisation LIM ou une séquence nucléotidique codant ladite protéine morphogénique osseuse ou protéine de minéralisation LIM; et 20

un minéral particulaire ayant une taille moyenne de particule d'environ 0,050 à environ 5,0mm, ledit minéral constituant au moins 20% en volume de ladite composition. 25

12. Composition selon la revendication 11, dans laquelle le minéral constitue environ 20% à environ 80% en volume de la composition. 30

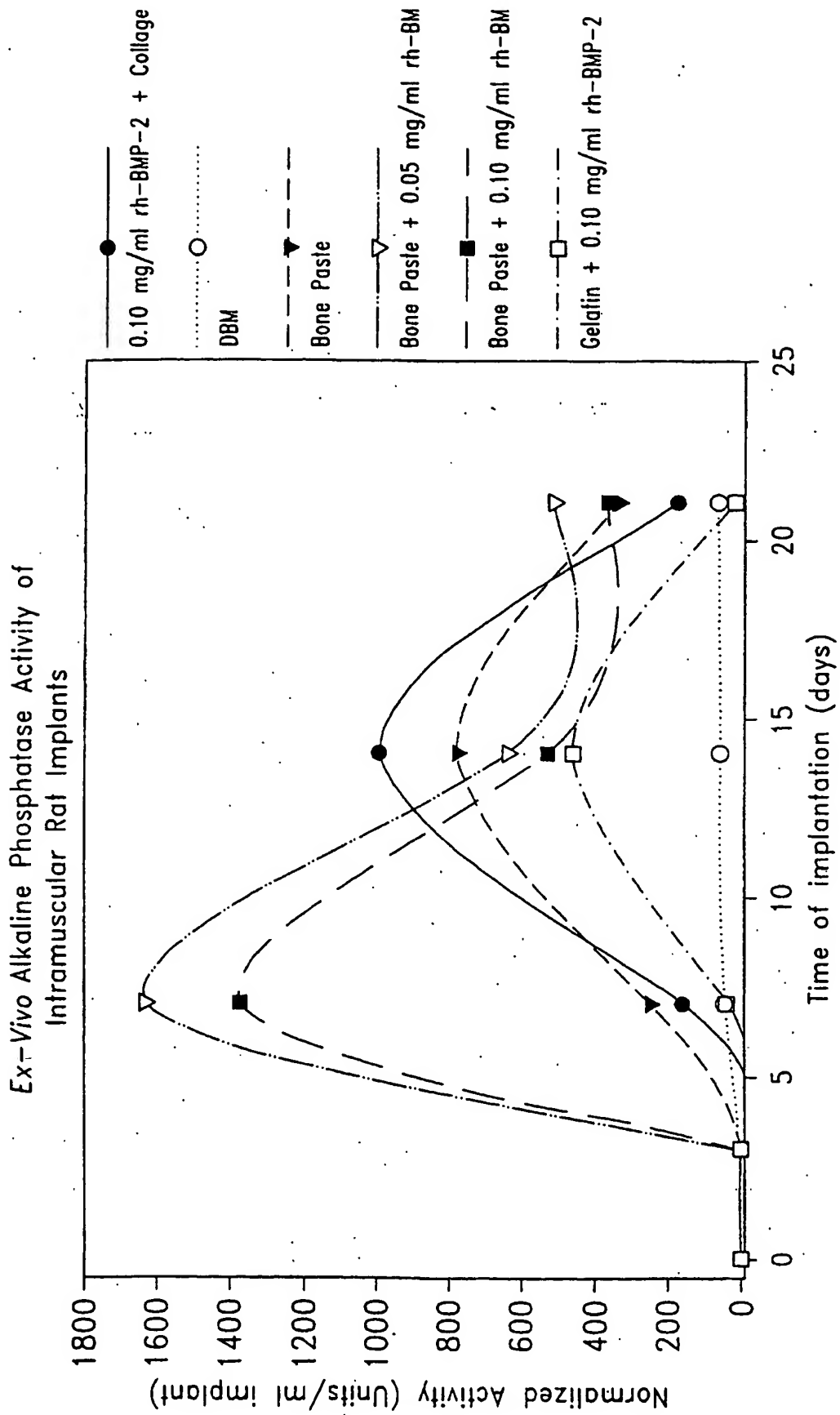
13. Composition selon la revendication 11, dans laquelle le minéral comprend des particules d'os humain. 35

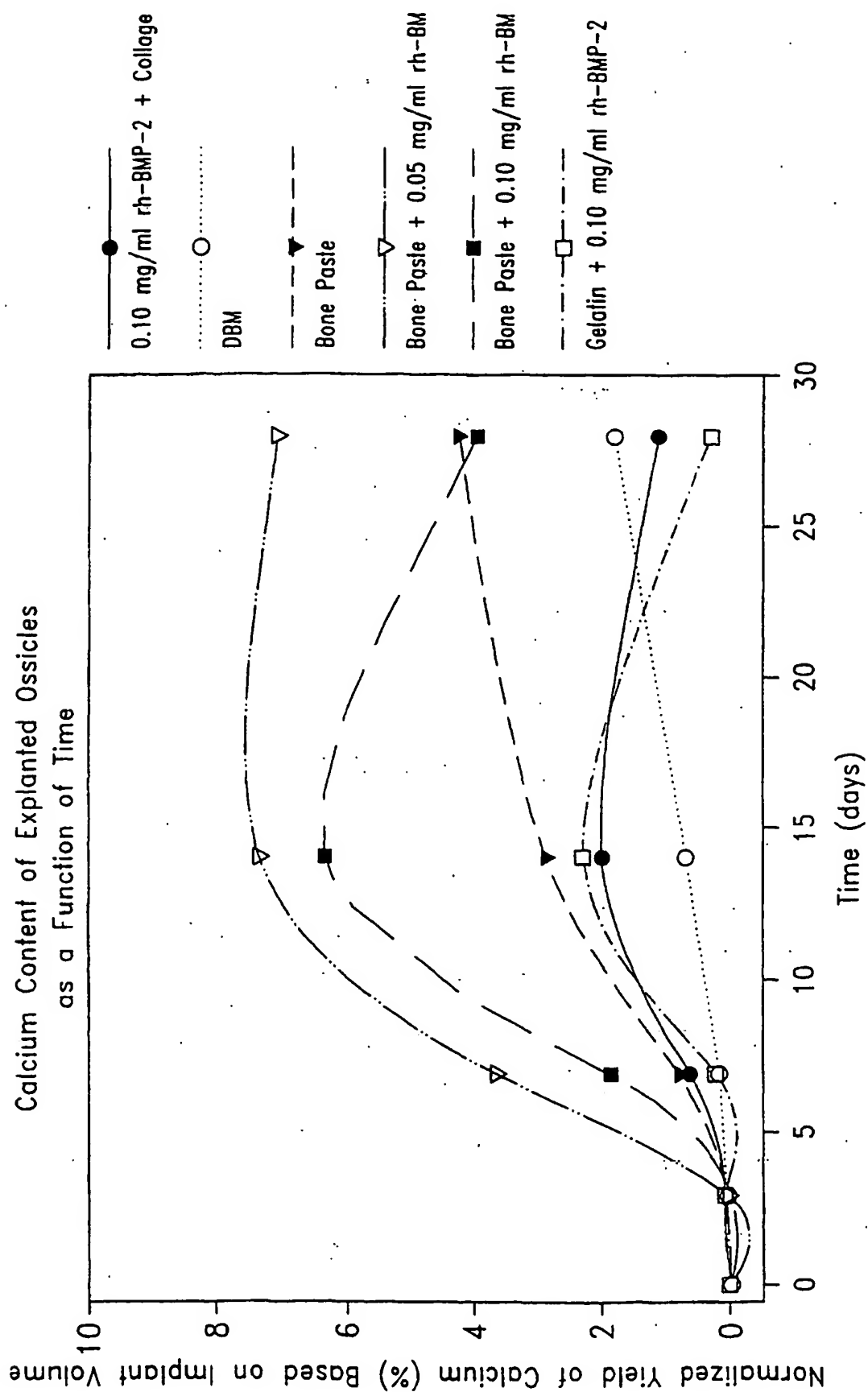
14. Composition selon la revendication 11, dans laquelle le minéral comprend des particules d'os non humain, lesdites particules ayant été traitées pour réduire leur immunogénicité chez les humains. 40

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**Fig. 1**

**Fig. 2**